



HAL
open science

Three-dimensional dispersion entropy for uterine fibroid texture quantification and post-embolization evaluation

Delphine Lebret, Andreia S. Gaudencio, Mirvana Hilal, Sonia Saib, Rakelle Haidar, Michel Nonent, Anne Humeau-Heurtier

► **To cite this version:**

Delphine Lebret, Andreia S. Gaudencio, Mirvana Hilal, Sonia Saib, Rakelle Haidar, et al.. Three-dimensional dispersion entropy for uterine fibroid texture quantification and post-embolization evaluation. *Computer Methods and Programs in Biomedicine*, 2022, 215, pp.article id. 106605. <10.1016/j.cmpb.2021.106605>. <hal-03503136>

HAL Id: hal-03503136

<https://univ-angers.hal.science/hal-03503136v1>

Submitted on 22 Jul 2024

HAL is a multi-disciplinary open access archive for the deposit and dissemination of scientific research documents, whether they are published or not. The documents may come from teaching and research institutions in France or abroad, or from public or private research centers.

L'archive ouverte pluridisciplinaire **HAL**, est destinée au dépôt et à la diffusion de documents scientifiques de niveau recherche, publiés ou non, émanant des établissements d'enseignement et de recherche français ou étrangers, des laboratoires publics ou privés.



Distributed under a Creative Commons CC BY-NC 4.0 - Attribution - Non-commercial use - International License

Three-dimensional dispersion entropy for uterine fibroid texture quantification and post-embolization evaluation*

Delphine Lebre^{a,b,*}, Andreia S. Gaudêncio^{a,c}, Mirvana Hilal^a, Sonia Saib^d, Rakelle Haidar^a, Michel Nonent^d and Anne Humeau-Heurtier^a

^aUniv Angers, LARIS, SFR MATHSTIC, F-49000 Angers, France.

^bPolytech Grenoble, Grenoble INP - Grenoble Alpes University, France.

^cLIBPhys, University of Coimbra, Portugal.

^dCHRU La Cavale Blanche, Brest, France.

ARTICLE INFO

Keywords:

entropy
magnetic resonance imaging
multiscale analysis
quality of life
texture
uterine fibroid embolization

ABSTRACT

Background and Objective: Uterine fibroids are benign tumors that could lead to symptoms complicating a patient's daily life. Those fibroids can be treated using uterine fibroid embolization (UFE), an effective non-surgical procedure. However, objectively quantifying the benefits of such a procedure, and the patient's quality of life, is rather challenging. **Methods:** With a novel multiscale three-dimensional (3D) entropy-based texture analysis, the multiscale 3D dispersion entropy (MDispEn_{3D}), this work aims to objectively quantify the evolution – after UFE – of patients' health in terms of quality of life, symptoms severity, and sexual function. For this purpose, clinical data and magnetic resonance imaging (MRI) scans of fibroids are analyzed before UFE (D0), ten days after (D10), and six months after (M6). **Results:** An inverse correlation is observed between MDispEn_{3D} entropy values and both size and volume of fibroids. An inverse correlation is also observed between MDispEn_{3D} at M6 and the scores of symptoms severity. Moreover, the patient age is found to be related to the relative difference of DispEn_{3D} and MDispEn_{3D} values, between D0 and M6, translating into an increasing entropy value. Furthermore, we show that history of fibroma plays a role in determining the obtained DispEn_{3D} values at D0. Finally, we observe that the lower MDispEn_{3D} values at D0, the larger the size of the fibroid at M6. **Conclusions:** The proposed MDispEn_{3D} method – by quantifying fibroid texture – could assist the medical doctors in the prognosis of uterine fibroids and the patients' quality of life assessment post-UFE. It could therefore favor the choice of this treatment compared to other more invasive surgical treatments.

1. Introduction

Uterine fibroids, also called leiomyomas, are benign tumors that grow in the uterus. Twenty to thirty percent (20%-30%) of women in their childbearing years are affected by this condition, half of them being asymptomatic [1, 2]. For the other half, symptoms degrade the quality of life, the sexual function, and can cause pelvic pain and heaviness, amenorrhea, menometrorrhagia, compression of nearby organs, infertility or even early miscarriage [1].

Fibroids are composed of muscular and fibrous tissues. Their location can be subserous, interstitial/intramural, or submucosal/intracavitary (International Federation of Gynaecology and Obstetrics classification) [3]. Their type can be non-degenerated or degenerated, non-degenerated oedematous, hypercellular, mixoid/cystic or "red" degeneration, and adenomyoma [4]. Moreover, the incidence of uterine fibroids is higher for women of dark skin, with a higher number of fibroids present and being of a larger size, and associated with more invalidating symptoms. There are also other dispositions to uterine fibroids such as diabetes, family history, nulliparity, obesity, and hypertension. So far, no genetic cause has been found for common uterine fibroids.

However, for rare uterine fibroids, such as multiple cutaneous and uterine leiomyomatosis, their occurrence has been attributed to genes encoding the mitochondrial enzyme, fumarate hydratase. In addition, it has been shown that the ovarian steroids estrogen and progesterin, growth factors, angiogenesis, and apoptosis processes are the primary regulators of fibroid growth [1, 2].

Patients suffering from uterine fibroids can use medication to reduce the symptoms or limit the evolution of the fibroid. Surgery is also possible to remove the fibroid (myomectomy) or the uterus (hysterectomy). Other procedures, such as uterine fibroid embolization (UFE), can also be proposed to either reduce or destroy the fibroid. UFE is a minimally invasive procedure in which the radiologist injects microspheres of hydrogel into the arteries that feed the fibroid. The goal is to block the fibroid influx. Since the 1990's, this procedure is used as an alternative to myomectomies and hysterectomies as it is safer and is associated with less complications [5].

In order to evaluate the benefits of UFE, surveys can be proposed to patients. These surveys are composed of scales and questions where the patients have to answer on a Likert scale. The latter includes five different answers that define the degree of strength, agreement, and frequency according to the questions asked (e.g., very high, high, medium, low, very low, or nonexistent). The answers are studied as ordinal variables. Spies et al. [6] proposed the so-called Uterine

*Funding sources here.

*Corresponding author

✉ delphine.lbt49@gmail.com (D. Lebre)

ORCID(s):

50 Fibroid Symptom and Quality Of Life (UFS-QOL) survey
 51 to determine a severity of symptoms (SSS) score and a
 52 quality of life (HRQL) score. A high SSS score indicates
 53 severe symptoms, while a high HRQL score indicates a
 54 good quality of life. From these scores, it has been reported
 55 that patients who undergo UFE have a significant change
 56 in their quality of life and symptoms severity 3 months
 57 after embolization [6]. Female sexual function index (FSFI)
 58 has also been proposed in [7]. FSFI evaluates the sexual
 59 function of women. It is composed of sub-scores such as
 60 desire, arousal, lubrication, orgasm, satisfaction, and pain. A
 61 high FSFI score represents good sexual function. However,
 62 a score below 26.55 indicates sexual dysfunction [7].

63 Although these surveys provide important information,
 64 once the UFE procedure is performed, it is still difficult
 65 for radiologists to *objectively quantify* the evolution of pa-
 66 tients' health and, thus, evaluate the patients' well being
 67 after embolization. In order to overcome this drawback,
 68 we herein propose, first, to quantify MRI fibroid texture
 69 through a novel multiscale tridimensional entropy-based
 70 algorithm. Texture of an image is related to the structure
 71 of its patterns. It has recently been shown that entropy-
 72 based measures can lead to interesting results for texture
 73 quantification [8, 9, 10, 11, 12] To the best of our knowledge,
 74 only two algorithms have been proposed for the analysis of
 75 three-dimensional data: the approximate entropy (ApEn3D)
 76 [13] and the fuzzy entropy (FuzEn3D) [14, 15]. In this
 77 work, we introduce the multiscale three-dimensional disper-
 78 sion entropy (MDispEn_{3D}) to evaluate the irregularity and
 79 complexity of uterine fibroids towards an assisted diagnosis.
 80 Second, in this study we also propose to study the relation
 81 between the entropy-based texture and patient quality of life
 82 as determined through the two above-mentioned surveys.
 83 Our results could therefore help the medical doctors in
 84 improving the patients' quality of life and performing better
 85 prognosis after UFE procedure.

86 The rest of the paper is organized as follows: the Ma-
 87 terials and Methods section introduces the new multiscale
 88 3D entropy-based algorithm, the synthetic data proposed
 89 for the algorithm validation, and the clinical data used. We
 90 also present the statistical tests performed. The results are
 91 detailed and analyzed in the Results and Discussion section.
 92 We finally end with a conclusion.

93 2. Materials and methods

94 2.1. Multiscale three-dimensional dispersion 95 entropy

96 To objectively quantify the evolution of patient health
 97 after UFE, we first propose to quantify the texture of vol-
 98 umetric MRI data. For this purpose, we introduce the ex-
 99 tension of the dispersion entropy (DispEn) [16] algorithm to
 100 3D data (DispEn_{3D}). Moreover, we also propose a multiscale
 101 approach for DispEn_{3D} (MDispEn_{3D}).

102 The DispEn algorithm [16] quantifies the irregularity
 103 of a signal by first mapping the signal into several classes
 104 (c classes). The mapping procedure can be performed

105 using linear or nonlinear techniques. For this purpose, the
 106 first step is to assign the signal, \mathbf{x} , elements with a value
 107 between 0 and 1, obtaining \mathbf{y} . Then, each element of \mathbf{y}
 108 is assigned an integer (from 1 to c). Once each element
 109 has its class defined, several vectors of m elements are
 110 obtained, where m is the embedding dimension. These
 111 vectors are called templates or embedding vectors and are
 112 basically a group of samples of the mapped signal with
 113 the assigned classes. Each of these templates are converted
 114 to dispersion patterns. Afterwards, the probability of each
 115 possible dispersion pattern is calculated. The final step is
 116 to obtain the entropy value using the Shannon's definition
 117 for these probability values [16]. The three-dimensional
 118 version, DispEn_{3D}, is very similar to DispEn, where
 119 the main differences are that the analysed data, \mathbf{U} , has
 120 three-dimensions, and therefore, the templates are no longer
 121 vectors but three-dimensional structures, and the mapped
 122 data will also be a volume, \mathbf{Y} .

123 Consider a volume \mathbf{U} of dimensions $H \times W \times L$, where
 124 H represents the height, W represents the width, and L
 125 the length, with its elements being $u_{i,j,k}$ for $1 \leq i \leq H$,
 126 $1 \leq j \leq W$, and $1 \leq k \leq L$.

127 First, each element $u_{i,j,k}$ is mapped with integers from 1
 128 to c classes. This procedure can be performed using linear
 129 or nonlinear approaches. To obtain DispEn_{3D}, the normal
 130 cumulative distribution function (NCDF) is used to perform
 the mapping procedure. Even though linear mapping can
 be fast, for a distribution of \mathbf{U} where the extreme values
 (maximum/minimum) are considerably larger than the med-
 ian or mean value, the mapping results in very few classes.
 In addition, some natural processes are known for having
 a sigmoid-based behavior [16, 17]. Therefore, the NCDF
 is used to map the volume \mathbf{U} to the new volume \mathbf{Y} . The
 elements $y_{i,j,k}$ of \mathbf{Y} are obtained as follows:

$$y_{i,j,k} = \frac{1}{\sigma\sqrt{(2\pi)}} \int_{-\infty}^{u_{i,j,k}} \exp\left(-\frac{(t-\mu)^2}{2\sigma^2}\right) dt, \quad (1)$$

128 where μ is the mean value of \mathbf{U} , σ is the standard deviation
 129 (SD) of \mathbf{U} , and $y_{i,j,k}$ is the element of the mapped volume \mathbf{Y}
 130 assuming a value between 0 and 1.

Afterwards, each $y_{i,j,k}$ is assigned to an integer value
 between 1 and c , obtaining the elements of \mathbf{Z} according to
 the following procedure:

$$z_{i,j,k}^c = \text{round}(c \times y_{i,j,k} + 0.5). \quad (2)$$

Then, the templates, $z^{c,m}(p, q, r)$, are obtained using
 the embedding dimension vector, $\mathbf{m} = [m_H, m_W, m_L]$, as
 follows:

$$\begin{aligned} z^{c,m}(p, q, r) &= \{z^c(p + \alpha, q + \beta, r + \gamma)\}, \\ &1 \leq \alpha \leq m_H - 1, \\ &1 \leq \beta \leq m_W - 1, \\ &1 \leq \gamma \leq m_L - 1, \end{aligned} \quad (3)$$

131 with $1 \leq p \leq H - m_H - 1$, $1 \leq q \leq W - m_W - 1$, and
 132 $1 \leq r \leq L - m_L - 1$. Therefore, the template can be defined

133 as a sub-sample of the volume. Afterwards, each template
 134 $z^{c,m}(p, q, r)$ is mapped to a dispersion pattern $\pi_{v_0, v_1, \dots, v_n}$ with
 135 $n = m_H \times m_W \times m_L - 1$, $v_0 = z^c(p, q, r)$, $v_1 = z^c(p+1, q, r)$,
 136 and $v_n = z^c(p + m_H - 1, q + m_W - 1, r + m_L - 1)$.

137 The number of possible dispersion patterns, n_z , for each
 138 template $z^{c,m}(p, q, r)$ is $n_z = c^{m_H \times m_W \times m_L}$. This number
 139 emerges due to the fact that the number of elements of a
 140 template is $m_H \times m_W \times m_L$, and each element is mapped as
 141 an integer number between 1 and c . The number of possible
 142 embedded dispersion patterns is $N_m = (H - m_H + 1) \times (W -$
 143 $m_W + 1) \times (L - m_L + 1)$.

For each potential dispersion patterns $\pi_{v_0, v_1, \dots, v_n}$, we
 obtain the relative frequency as follows:

$$p(\pi_{v_0, \dots, v_n}) = \frac{\#\{p, q, r | z^{m,c}(p, q, r) \text{ has type } \pi_{v_0, \dots, v_n}\}}{N_m}, \quad (4)$$

144 with $p \leq H - m_H - 1$, $q \leq W - m_W - 1$, and $r \leq L - m_L -$
 145 1 . The probability $p(\pi_{v_0, \dots, v_n})$ corresponds to the number
 146 of dispersion patterns of $\pi_{v_0, v_1, \dots, v_n}$ for its corresponding
 147 template $z^{m,c}(p, q, r)$ within the total number of possible
 148 embedded templates N_m .

Then, using the Shannon's entropy definition, DispEn_{3D}
 is obtained as:

$$\text{DispEn}_{3D}(\mathbf{U}, m, c) = - \sum_{\pi=1}^{n_z} p(\pi_{v_0, \dots, v_n}) \times \ln(p(\pi_{v_0, \dots, v_n})). \quad (5)$$

149 As an illustration, consider the volume in Figure 1 with
 150 4 voxels height, 3 voxels width, and 2 voxels length. The
 151 values of each $H \times W$ matrix within the length of the volume
 152 are also shown in Figure 1. According to the DispEn_{3D}
 153 algorithm, the first step is to obtain the volume \mathbf{Y} based on
 154 the NCDF mapping (Figure 2). Then, each voxel is rounded
 155 according to Equation 2. In this case, if we define the number
 156 of classes as $c = 3$, this leads to the volume shown in Figure
 157 3. Then, we have to create the templates. For the purposes
 158 of this example, we define the embedding dimension as $\mathbf{m} =$
 159 $[2, 2, 2]$. In Figure 4, we can observe that the first template
 160 $z^{c,m}(1, 1, 1)$ corresponds to the voxels in pink and the second,
 161 $z^{c,m}(1, 2, 1)$, corresponds to the blue ones.

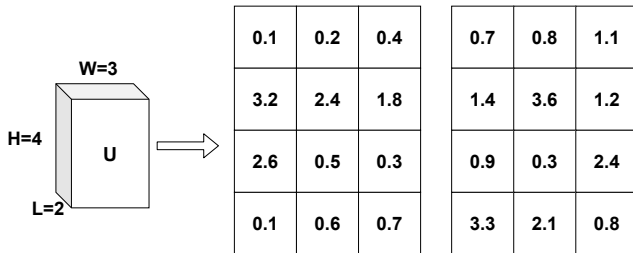


Figure 1: Example of a volume \mathbf{U} with $H = 4$, $W = 3$, and $L = 2$ (left), with the corresponding values for each layer within the length of the volume (right).

162 The number of possible templates for the established \mathbf{m}
 163 is $N_m = (4 - 2 + 1) \times (3 - 2 + 1) \times (2 - 2 + 1) = 6$.

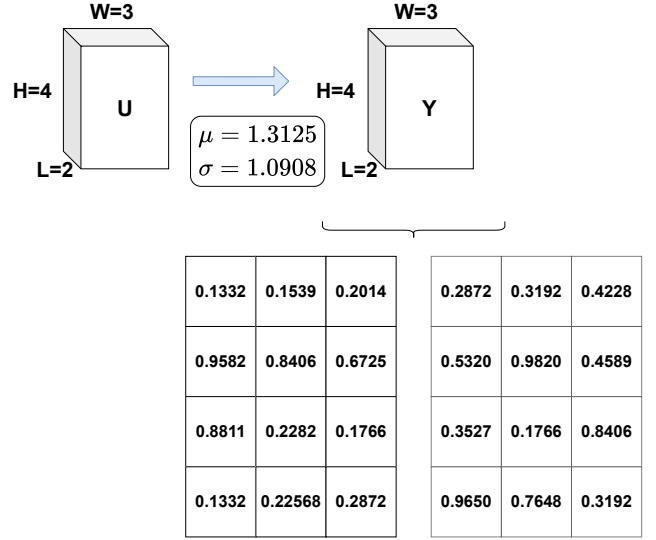


Figure 2: Volume \mathbf{Y} (right at the top) obtained after the mapping procedure of volume \mathbf{U} (presented in Figure 1), with mean and SD values of $\mu = 1.3125$ and $\sigma = 1.0908$, respectively, and the corresponding values for each layer within the length of \mathbf{Y} (bottom).

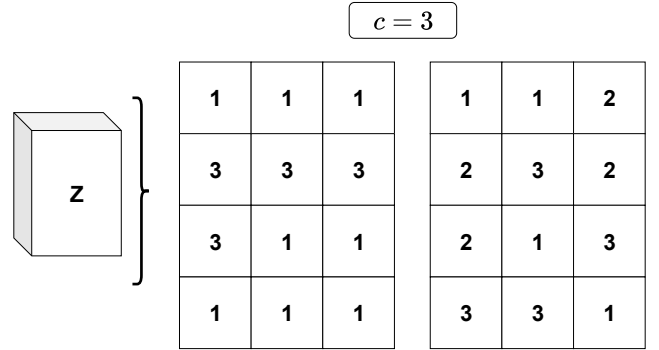


Figure 3: Volume \mathbf{Z} obtained after the rounding operation of the elements of \mathbf{Y} shown in Figure 2, for $c = 3$.

In this case, none of the dispersion patterns obtained repeats
 164 itself. Therefore, the probability of each pattern is $1/6$. After
 165 applying the Shannon definition, for this example, we verify
 166 that the entropy value using DispEn_{3D} is 1.7918.
 167

Costa et al. [18] suggested the use of a multiscale analy-
 168 sis to evaluate the irregularity of biomedical systems through
 169 multiple temporal scales. This approach, originally applied
 170 to signals, is based on a coarse-graining procedure where the
 171 signal is down-sampled using an averaging method for mul-
 172 tiple scale factors (τ). By extending the original procedure
 173 to three-dimensions, for a volume \mathbf{U} , the new coarse-grained
 174 volume $\mathbf{Y}^{(\tau)}$ is obtained as follows:
 175

$$\mathbf{Y}_{i,j,k}^{(\tau)} = \frac{1}{\tau^3} \sum_{\substack{l=(i-1)\tau+1 \\ m=(j-1)\tau+1 \\ n=(k-1)\tau+1}}^{k\tau} \mathbf{U}_{l,m,n}, \quad (6)$$

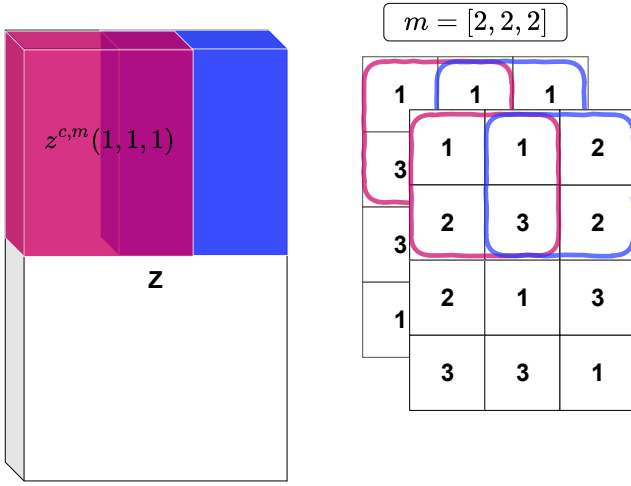


Figure 4: Representation of the embedded templates for $\mathbf{m} = [2, 2, 2]$ of the volume \mathbf{Z} .

was composed of periodic images as shown in Figure 5 (a), (b), and (c), while the second group was composed of non-periodic images as shown in Figure 5 (d), (e), and (f). An algorithm generates these textures using a deterministic search process where each region of the periodic texture is equivalent to that of the non-periodic texture [20]. This algorithm is based on Markov random field texture models. To compute DispEn_{3D} values, the parameters were set as $c = 5$, and $\mathbf{m} = [2, 2, 2]$. These parameters were used previously for 1D data in [16, 21]. This test will allow to illustrate if the DispEn_{3D} algorithm is able to differentiate texture behaviors.

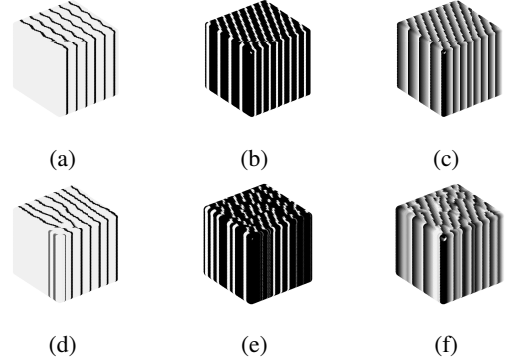


Figure 5: Volumes of $256 \times 256 \times 256$ voxels presenting periodic textures (a), (b), and (c), and their non-periodic textures (d), (e), and (f) based on the textures of [22].

where τ is the scale factor, determining the rate of down-sampling, $1 \leq l \leq H/\tau$, $1 \leq m \leq W/\tau$, and $1 \leq n \leq L/\tau$, and the volume $\mathbf{Y}^{(\tau)}$ has $\frac{H}{\tau} \times \frac{W}{\tau} \times \frac{L}{\tau}$ voxels. For example, if a volume \mathbf{U} has $100 \times 100 \times 100$ voxels, for $\tau = 1$, $\mathbf{Y}^{(1)} = \mathbf{U}$, for $\tau = 2$, the volume $\mathbf{Y}^{(2)}$ will have half of the length, half of the width, and half of the height, having therefore, $50 \times 50 \times 50$ voxels, and for $\tau = 3$, $\mathbf{Y}^{(3)}$ will have a third of the length, a third of the width, and a third of the height, *i.e.*, $33 \times 33 \times 33$ voxels, and so on.

When using a multiscale approach, several τ values are used, leading to several coarse-grained versions of the original volume. Then, the entropy measure (in this case DispEn_{3D}) is applied to each coarse-grained volume, leading to the multiscale approach (in this case, $M\text{DispEn}_{3D}$) to evaluate the complexity of a biomedical data. The maximum scale factor determines the size of the smallest down-sampled volume. Due to the size of our data, the maximum τ value was chosen equal to 6. For our analysis, the DispEn_{3D} entropy values were thus analyzed for $1 \leq \tau \leq 6$. Besides, a new variable θ was defined based on the sum of these $M\text{DispEn}_{3D}$ values:

$$\theta = \sum_{\tau=1}^6 M\text{DispEn}_{3D}(\tau), \quad (7)$$

where $M\text{DispEn}_{3D}(\tau)$ corresponds to the multiscale entropy value obtained for the scale factor τ using DispEn_{3D} as the entropy measure. The algorithms were executed using MATLAB®.

2.2. Validation tests

We performed several tests for the proposed algorithms to validate their ability on identifying increasing irregularity degrees and verify their proper behavior with 3D data. DispEn_{3D} was tested on different cubes of dimensions $256 \times 256 \times 256$ voxels. These volumes are composed of images taken from [19]. The first group of synthetic textures

2.3. Clinical data

The magnetic resonance imaging (MRI) scans were obtained from 42 patients who went through UFE (at 3 time instances for the follow-up), in the Centre Hospitalier Regional Universitaire (CHRU) La Cavale Blanche and the Polyclinique Keraudren, both in Brest, between 2018 and 2020. Consent was obtained from the patients and the work has been approved by the ethical committee. The study of MRI scans was performed for sagittal T2 scans without gadolinium as recommended by the medical doctors. The average age of the patients was 45 ± 9 years, that is goes back to the most common age of the onset of fibroids [1, 2]. This study included the UFS-QOL and FSFI surveys. The patients had to complete these surveys at 3 time instances: the day of the UFE procedure (D0), after 10 days (D10), and after six months (M6). The protocol was carried out by an experienced radiologist (Pr. M.N.). The patients underwent the procedure under local anesthesia. The embolization was realized with Embosphere®. The definition of the region of interest (ROI) was performed by Dr. S.S., a radiology intern; the volume of the fibroid and the apparent diffusion coefficient (ADC) were computed. ADC is related to the degree of water diffusion in tissues [23].

Several variables were studied, including clinical and image-based features. The clinical data included the following: age, body mass index (BMI), gestiture, parity, number of spontaneous miscarriages, presence of a previous fibroid,

247 type of contraception used, treatment taken by the patient
 248 before embolization (D0), and the scores obtained from the
 249 surveys (FSFI, SSS, and HRQL) at D0 and M6. From the
 250 fibroid, characteristics like volume and ADC were also con-
 251 sidered at D0, D10, and M6. These variables were defined
 252 as being related either to the appearance of a fibroid or its
 253 evolution.

254 The MRI scans were evaluated using $MDispEn_{3D}$. The
 255 size of the main fibroid was identified with the medical
 256 doctors. To determine the volume to process, first a square
 257 containing the ROI was determined by the radiologist and
 258 defined on an equal volume regardless of the MRI acqui-
 259 sition instant for each patient (see Figures 6 and 7). Then, the
 260 number of processed images (z-dimension) was considered
 261 to be the minimum number of images composing each
 262 patient's MRI scans (D0, D10, M6). The smallest volume
 263 of interest (VOI) considered in the study had a dimension
 264 of $46 \times 46 \times 28$ voxels and the largest had a dimension of
 265 $233 \times 233 \times 28$ voxels. The size of fibroid was obtained using
 266 the major axis of the fibroid (see Figure 6).

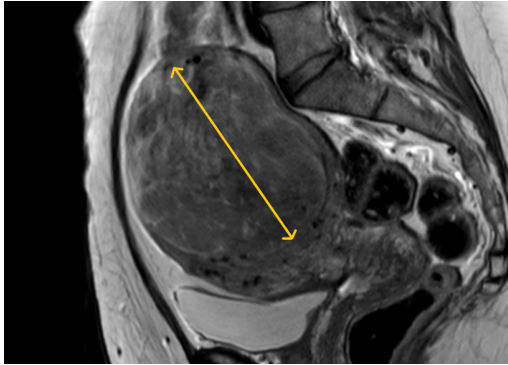


Figure 6: MRI scan of a patient with the definition of the size of the fibroid (yellow arrow).

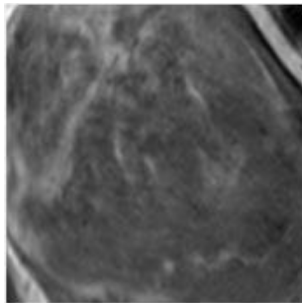


Figure 7: Squared ROI defined according to the MRI shown in Figure 6.

267 The ROI was then normalized to obtain a comparable
 268 average gray level among the MRI scans. The normalization
 269 procedure was performed as follows:

$$\mathbf{V}_{norm} = \frac{\mathbf{V} - \min(\mathbf{V})}{\max(\mathbf{V}) - \min(\mathbf{V})}, \quad (8)$$

270 where \mathbf{V} is the VOI containing the original ROI selected by
 271 the radiologist of a patient at one time period (D0, D10, or
 272 M6), $\min(\mathbf{V})$ corresponds to the minimum value of \mathbf{V} , and
 273 $\max(\mathbf{V})$ to the maximum value of \mathbf{V} .

274 The entropy of the VOI was calculated using the
 275 $MDispEn_{3D}$ algorithm, with the following parameters: num-
 276 ber of classes $c = 5$, embedding dimension $\mathbf{m} = [2, 2, 2]$,
 277 and the maximum τ value was chosen equal to 6. We have
 278 chosen the same parameters (number of classes, embedding
 279 dimensions, and τ) as in the texture validation test, recom-
 280 mended for 1D data [16, 21]

2.4. Statistical analysis

281 When analyzing entropy curves, all of the 42 patients
 282 were included in the analysis. When analyzing the survey
 283 answers and the entropy for correlation analysis, we only
 284 used 34 patients as 8 of them did not complete the sur-
 285 veys. After obtaining the 30 variables from the surveys, a
 286 descriptive statistical analysis was performed using the R[®]
 287 software. The minimum, maximum, and average values of
 288 each variable were considered. In addition, the normality and
 289 variance of these variables were verified using graphics. The
 290 normality assessment was performed using the *Shapiro-Wilk*
 291 test with a statistical significance of $\alpha = 0.05$.

We define the relative difference (RD) between D0 and
 M6 as:

$$RD_1(X) = \frac{X_{M6} - X_{D0}}{X_{D0}}, \quad (9)$$

293 where X is the variable under study, X_{D0} corresponds to the
 294 variable X before the embolization at D0, and X_{M6} is the
 295 variable X six months after embolization.

296 Similarly, we also define the relative difference of a
 297 variable between D0 and D10 as:

$$RD_2(X) = \frac{X_{D10} - X_{D0}}{X_{D0}}. \quad (10)$$

298 For all the statistical tests, the threshold of statistical
 299 significance was $\alpha = 0.05$.

300 The identification of a relationship between several con-
 301 tinuous quantitative variables was performed using the *Pear-*
 302 *son's* correlation coefficient (parametric) test or the *Spear-*
 303 *man's* correlation coefficient (non-parametric) test. For a
 304 p -value lower than the significance level, the correlation
 305 was accepted, rejecting the null hypothesis, and the cor-
 306 relation coefficients were retained. Then, the explanatory
 307 variables with normal distribution were studied using linear
 308 regression. For the variables that did not follow the normal
 309 distribution, a logarithmic transformation or using Box-Cox
 310 was used.

311 The variables with a normal distribution were used to
 312 explain the difference of the mean values between two
 313 samples. When the samples had the same variance values,
 314 the Student's test was performed. Otherwise, the *Welch's* test
 315 was implemented. Through the *Fisher's* test, the equality of
 316 variance between two samples was also verified.

Table 1

DispEn_{3D} values on the volumes composed by periodic textures (a), (b), and (c), and non-periodic textures (d), (e), and (f) shown in Figure 5.

Texture (a)	Texture (b)	Texture (c)
1.07	1.13	2.34
Texture (d)	Texture (e)	Texture (f)
1.14	1.20	2.58

Table 2

Correlation coefficient (ρ) and p -value (* means significant value) between the entropy values (scale factor $\tau = 1$ and θ) and the fibroid characteristics (size, volume, and ADC).

Variables	$\tau = 1$		θ	
	ρ	p -value	ρ	p -value
Size	-0.484	1.21×10^{-8} *	-0.498	4.12×10^{-9} *
Volume	-0.390	6.14×10^{-5} *	-0.452	2.34×10^{-6} *
ADC	-0.281	0.01*	-0.077	0.46

When testing more than two samples, the equality of variances was analyzed. The mean values were compared with the ANOVA (parametric) test or the *Kruskal-Wallis* (non-parametric) test. In case of a significant result for the ANOVA test, when having a control group, we used the *Dunn*'s test. This test identifies which sample is different from the control group. When a control group did not exist, the *Tukey*'s test was performed. For a significant result when using the *Kruskal-Wallis*, we used the *Dunn*'s test. The latter allows testing each sample against each of the remaining samples, and verifies when they are different.

When the quantitative variables did not have a Gaussian distribution, the number of (independent) samples of the qualitative variable was determined. For two samples, the non-parametric Wilcoxon signed rank test was used. For more than 2 samples, the *Kruskal-Wallis* test was used. For a significant result, the *Dunn*'s test allowed determining which sample allows the difference.

In order to verify the independence of two categorical variables, the χ^2 test of independence was used if at least 80% of the expected frequencies were greater than 5, with *Yates*'s correction. Otherwise, the *Fisher*'s exact test was used.

After evaluating the correlation between variables, if the correlation was found to be statistically significant (p -value < 0.05), linear regression models were performed.

3. Results and Discussion

3.1. Synthetic data

In Table 1, we can observe that the periodic synthetic-based volumes (Figures 5(a) and (b)) show lower DispEn_{3D} values than the non-periodic synthetic-based volumes (Figures 5(c) and (d)), as expected. Since the volumes (c) and (d) are more irregular than the volumes (a) and (b), their entropy values are higher. This leads to the conclusion that DispEn_{3D} has the ability to identify different irregularity degrees. In addition, volume (a) has larger variations and more gray content than volume (b). Therefore, its irregularity is higher. It should therefore lead to a higher entropy value. For similar reasons, volume (c) should lead to a higher entropy value than volumes (b) and (d). From Table 1, we observe that DispEn_{3D} has the ability to differentiate such textural behaviors.

3.2. Clinical data

As mentioned above, the MRI scans of uterine fibroids were assessed using MDispEn_{3D}. For this work, 6 scale

factors were studied and used in the computation of the θ score (see Equation 7).

Figure 8 shows the mean and standard deviation (SD) of the entropy values obtained for our dataset for each scale factor at D0, D10, and M6. We observe increasing entropy values with scale factors. This is true for entropy values computed at D0, D10, and M6. This can be explained by the fact that, when increasing the scale factor, the degree of down-sampling increases, and therefore, the resulting samples become less similar between each other. Given the lower similarity between samples, a more irregular down-sampled volume is obtained. When volumes are more irregular, the entropy is expected to be higher. Hence, in Figure 8, the entropy value is higher for larger scale factors since the irregularity increases with the down-sampling procedure.

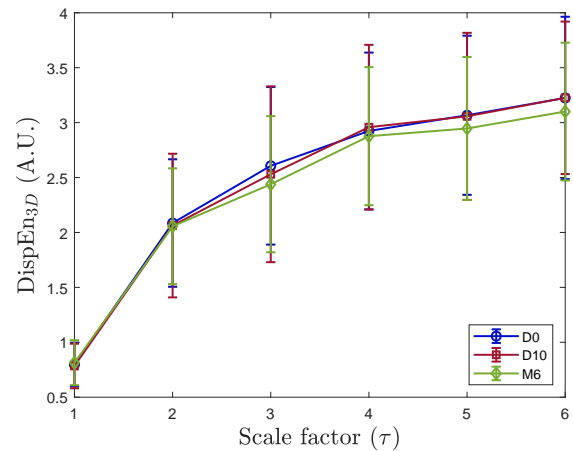


Figure 8: Mean and standard deviation values of MDispEn_{3D} for D0, D10, and M6, for $c = 5$, $\mathbf{m} = [2, 2, 2]$, and $1 \leq \tau \leq 6$.

Afterwards, we studied the possible correlation between the 30 variables. As shown in Table 2, significant inverse correlations were found between DispEn_{3D} value (at scale factor $\tau = 1$ and θ) and the fibroid size, between DispEn_{3D} values and fibroid volume, and between DispEn_{3D} at scale factor $\tau = 1$ and the ADC variable, for the periods D0, D10, and M6. These results are interesting as they reveal a direct relation between entropy values and the size and volume of the fibroid and, therefore, the evolution of the patient response to treatment.

Moreover, an inverse correlation was found between DispEn_{3D} values (at scale factor $\tau = 1$ and θ) and the SSS

score at M6: coefficient of -0.459 and a significant p -value of 8.16×10^{-3} for DispEn_{3D} at $\tau = 1$, and a coefficient of -0.488 and a significance of 4.60×10^{-3} for the θ score. As mentioned above, the SSS score is obtained using surveys to assess the severity of the symptoms. Our results show that, the higher the SSS score, the lower the DispEn_{3D} values at scale factor $\tau = 1$ or θ . DispEn_{3D} and its multiscale version therefore allow to objectively quantify the severity of the symptoms.

A positive correlation between the patients age and the relative difference of DispEn_{3D} (between D0 and M6) for $\tau = 1$ was also found to be significant with a confidence of 99% ($\rho = 0.43$ and $\alpha = 8.39 \times 10^{-3}$): for older patients a higher relative difference of entropy values is observed.

As mentioned above, when significant correlations were found between variables, we proceeded to model linear regressions. We thus obtained the following linear expression:

$$y_1 = 1.07 - 0.04 \times x_1, \quad (11)$$

where y_1 represents the DispEn_{3D} entropy value at scale factor $\tau = 1$, and x_1 represents the size of the fibroma (size of the major axis of the ROI), both regardless the period, as shown in Figure 9. Nearly 28% of the variance is expressed by this regression model.

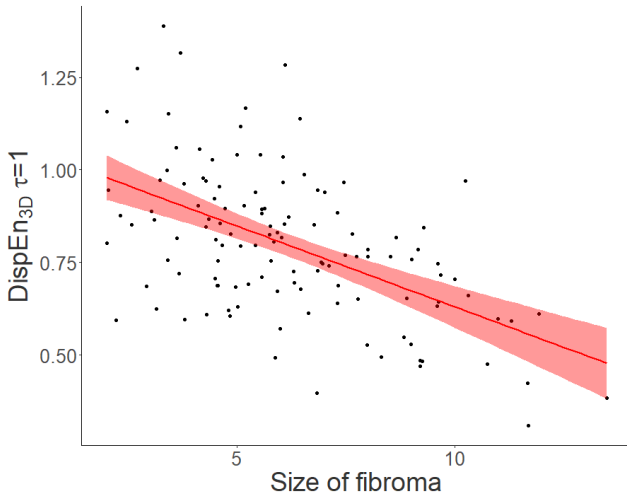


Figure 9: Linear regression between DispEn_{3D} at scale factor $\tau = 1$ using the size of the major axis of the fibroid.

A linear regression between θ and the size of the fibroma was also found:

$$y_2 = 18.81 - 0.70 \times x_2, \quad (12)$$

where y_2 represents the θ score and x_2 represents the size of the fibroma. Both variables were studied independently of the time instant (D0, D10, or M6).

Based on the relationship between the texture analysis and the fibroid major axis sizes, the evolution at M6 of fibroid size was modeled using DispEn_{3D} at scale factor $\tau = 1$ and at D0 according to the following expression:

$$\log(y_3) = 2.62 - 0.06 \times x_3, \quad (13)$$

where y_3 represents the size of fibroma at M6, and x_3 corresponds to the θ value at D0.

We also found a similar equation for $\tau = 1$ at D0:

$$\log(y_4) = 2.54 - 1.03 \times x_4, \quad (14)$$

where y_4 represents the size of fibroma at M6 and x_4 corresponds to the DispEn_{3D} value at scale factor $\tau = 1$, at D0. This model explains almost 28.0% of the variance. Multiscale entropy, using the θ score, allows explaining slightly more variance (30.0% against 28.0%), see Figure 10.

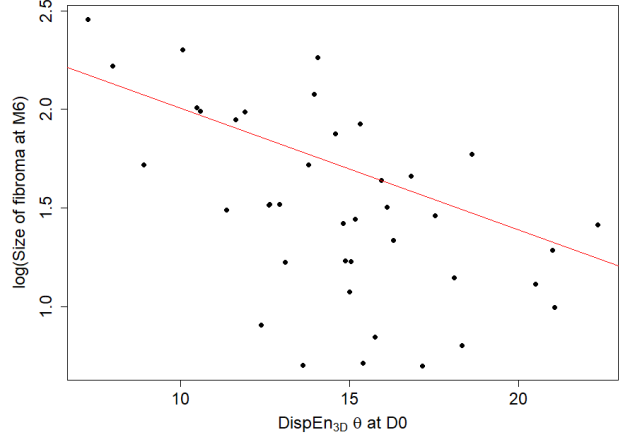


Figure 10: Linear regression explaining the size of fibroid at M6 using the θ score at D0.

Figure 11 shows the linear regression between DispEn_{3D} at $\tau = 1$ and the volume of the fibroid, regardless of the time period:

$$y_5 = 0.90 - (7.2 \times 10^{-4}) \times x_5, \quad (15)$$

where y_5 represents DispEn_{3D} at scale factor $\tau = 1$ and x_5 represents the volume of the fibroid at any period. A negative coefficient was found for this model, which was able to explain 25% of the variance. Even though size and volume are related, the size actually allows to obtain a slightly better value of explained variance.

A similar equation was found for θ and the volume of the fibroid independently of the time period:

$$y_6 = 16.23 - 0.01 \times x_6, \quad (16)$$

where y_6 represents the relative difference of θ (see Equation 7) between D0 and M6, and x_6 represents the volume of the fibroid.

The evolution of the texture (DispEn_{3D} at scale factor $\tau = 1$) between D0 and M6 was also determined using the patient age:

$$y_7 = -1.13 - 0.03 \times x_7, \quad (17)$$

where y_7 corresponds to the relative difference of DispEn_{3D} at $\tau = 1$ between M6 and D0 (see Equation 9) and x_7 represents the age of the patient.

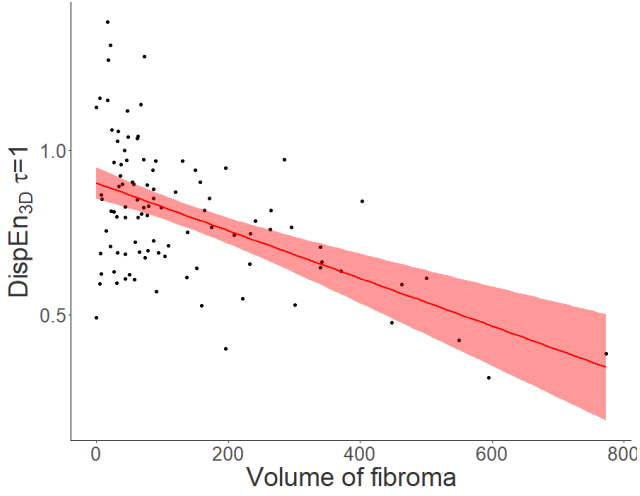


Figure 11: Linear regression between DispEn_{3D} at scale factor $\tau = 1$ and the fibroid volume.

430 A positive correlation between the age of the patient and
 431 the evolution of DispEn_{3D} at scale factor $\tau = 1$ between D0
 432 and M6 was found with a p -value of 0.01, see Figure 12. This
 433 means that older patients are expected to have higher positive
 434 evolution of texture, i.e., the relative difference between
 435 DispEn_{3D} values at D0 and M6 is expected to increase.
 436 This can be explained by the fact that older patients may
 437 have more often calcified fibroids, and the cessation of blood
 438 supply may result in a more significant change in texture than
 439 in younger patients. In fact, calcifications are present during
 440 the terminal phases of hyaline degeneration [24].

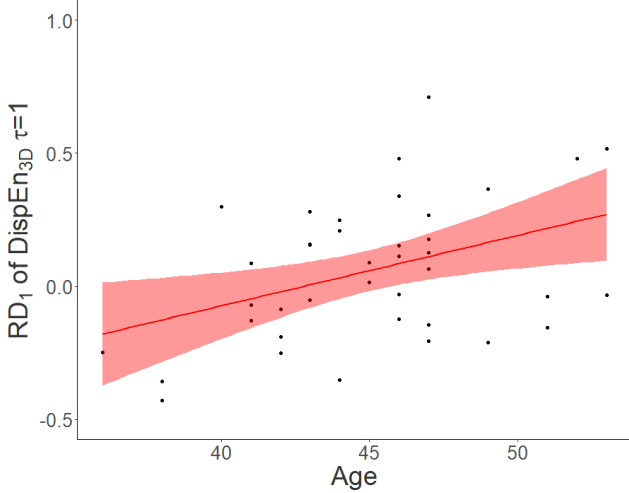


Figure 12: Linear regression between $RD_1(\text{DispEn}_{3D, \tau=1})$ and the age of the patient.

A linear regression between DispEn_{3D} at scale factor $\tau = 1$ and the SSS score, at M6, was also found:

$$y_8 = 0.09 - 0.01 \times x_8, \quad (18)$$

441 where y_8 represents DispEn_{3D} at scale factor $\tau = 1$ and at
 442 M6, and x_8 is the SSS score at M6.

Eq.	Variable x	Variable y	R^2	p -value
11	Size	$\tau = 1$	0.280	1.58×10^{-10}
12	Size	θ	0.251	1.86×10^{-9}
13	θ at D0	Size at M6	0.300	1.48×10^{-4}
14	$\tau=1$ at D0	Size at M6	0.280	2.67×10^{-4}
15	Volume	$\tau=1$	0.252	6.29×10^{-8}
16	Volume	θ	0.239	1.74×10^{-7}
17	Age	$RD_1(\tau = 1)$	0.142	9.66×10^{-3}
18	SSS at M6	$\tau=1$ at M6	0.161	0.01
19	SSS at M6	θ at M6	0.108	0.04

Table 3

R^2 and p -value of linear regressions obtained, equations 11 to 19.

In Figure 13 we observe that the lower the SSS score, the higher the DispEn_{3D} values, for a 98% confidence level. This relationship shows that it is possible to quantify *objectively* the SSS score.

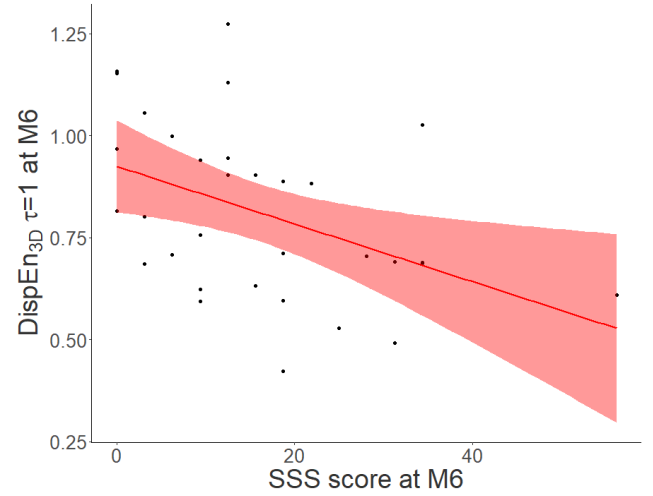


Figure 13: Linear regression between DispEn_{3D} at scale factor $\tau = 1$ and the SSS score, both at M6.

Similarly, the θ and the SSS score, both at M6, are modeled by:

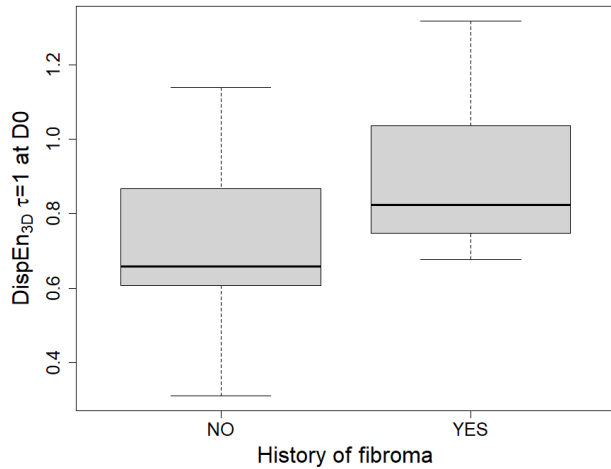
$$y_9 = 15.55 - 0.08 \times x_9, \quad (19)$$

where y_9 represents the θ variable as shown in equation 7 at M6, and x_9 represents the SSS score at M6. However, this model only explains about 11% of variance.

In table 3 we summarize the linear regression models and their R^2 coefficients as well as their p -values. As we can observe, all of the linear models were found to be statistically significant for $p < 0.05$. Moreover, 7 out of the 9 models were statistically significant for $p < 0.01$.

Finally, from Figure 14, we observe that the group of patients that had previous history of fibroids has a higher entropy value (scale factor $\tau = 1$). The texture of fibroids between the group of patients that had previous history of fibroids and the group that did not is statistically different (p -value= 0.02). Therefore, the texture of a fibroid before

461 surgery might be modified with the presence of previous
462 history of fibroid.



463 **Figure 14:** Boxplot representing DispEn_{3D} values (for scale
464 factor $\tau = 1$) according to previous history of fibroid (YES)
465 or not (NO).

463 4. Conclusion

464 In this paper we introduced the multiscale tridimensional
465 dispersion entropy (MDispEn_{3D}). It was applied on MRI
466 scans of uterine fibroids. One of the main results of this study
467 is the prediction, before EFU, with a 99% confidence level,
468 of the size of the fibroid 6 months after the embolization.
469 Additionally, this study reveals inverse correlations between
470 the 3D texture of uterine fibroids, using MDispEn_{3D} , and
471 their morphological characteristics (like size and volume).
472 These linear regressions show a confidence level higher than
473 99%. Moreover, the older patients show a larger positive
474 difference in entropy values. The associated model has a
475 confidence level higher than 99% and may be a positive
476 indication that EFU is efficient for these patients who may
477 have an additional benefit through this treatment.

478 We also have *objectively* quantified the severity of the
479 patients symptoms using 3D texture analysis at M6. The
480 answers to the symptom severity survey remain subjective,
481 as sometimes the tolerance of the patient might influence her
482 response. Texture analysis might be a good alternative to the
483 SSS score evaluation at M6. Besides, MDispEn_{3D} may be an
484 interesting tool to help medical doctors towards a quantifica-
485 tion of the evolution of fibroids characteristics after EFU. It
486 could also help in identifying if EFU is appropriate for the
487 patient, as mentioned for the older women. If the response
488 is negative, another treatment could be considered by the
489 doctor.

490 There is still space to improve this study as it would be
491 interesting to include patients with additional characteristics
492 such as patients with different ethnicity, patients experienc-
493 ing menopause, or other elements related to the evolution of
494 fibroids.

CRedit authorship contribution statement

495 **Delphine Lebret:** Conceptualization of this study, Me- 496
497 thodology, Software, Formal Analysis, Writing - Original
498 Paper, Writing - Review and Editing.. **Andreia S. Gaudên- 499**
500 **cio:** Methodology, Software, Formal Analysis, Writing -
501 Original Paper, Writing - Review and Editing. **Mirvana 502**
503 **Hilal:** Supervision, Conceptualization of this study, Metho-
504 dology, Formal Analysis, Writing - Review and Editing.
505 **Sonia Saib:** Conceptualization of this study, Methodology,
506 Resources, Writing - Review and Editing. **Rakelle Haidar:**
507 Methodology, Software. **Michel Nonent:** Conceptualization
508 of this study, Methodology, Resources, Writing - Review
509 and Editing. **Anne Humeau-Heurtier:** Supervision, Con-
ceptualization of this study, Methodology, Formal Analysis,
Writing - Review and Editing.

References

- 510
- 511 [1] S. Gupta, J. Jose, I. Manyonda, Clinical presentation of fibroids, Best
512 practice & research Clinical obstetrics & gynaecology 22 (2008) 615–
513 626.
 - 514 [2] S. Okolo, Incidence, aetiology and epidemiology of uterine fibroids,
515 Best practice & research Clinical obstetrics & gynaecology 22 (2008)
516 571–588.
 - 517 [3] M. G. Munro, H. O. Critchley, M. S. Broder, I. S. Fraser, for the FIGO
518 Working Group on Menstrual Disorders, Figo classification system
519 (palm-coein) for causes of abnormal uterine bleeding in nongravid
520 women of reproductive age, International Journal of Gynecology &
521 Obstetrics 113 (2011) 3–13.
 - 522 [4] H. Ueda, K. Togashi, I. Konishi, M. L. Kataoka, T. Koyama, T. Fu-
523 jiwara, H. Kobayashi, S. Fujii, J. Konishi, Unusual appearances
524 of uterine leiomyomas: Mr imaging findings and their histopathologic
525 backgrounds, RadioGraphics 19 (1999) S131–S145. PMID:
526 10517450.
 - 527 [5] A. M. White, J. B. Spies, Uterine fibroid embolization, Techniques
528 in Vascular and Interventional Radiology 9 (2006) 2–6.
 - 529 [6] J. B. Spies, K. Coyne, N. G. Gwaou, D. Boyle, K. Skymarz-Murphy,
530 S. M. Gonzalez, The ufs-qol, a new disease-specific symptom and
531 health-related quality of life questionnaire for leiomyomata, Obstet-
532 rics & Gynecology 99 (2002) 290–300.
 - 533 [7] M. Sand, R. Rosen, C. Meston, L. Brosso, The female sexual func-
534 tion index (fsfi) : a potential "gold standard" measure for assessing
535 therapeutically-induced change in female sexual function, Fertility
536 and Sterility 92 (2009) S129.
 - 537 [8] C. Morel, A. Humeau-Heurtier, Multiscale permutation entropy for
538 two-dimensional patterns, Pattern Recognition Letters 150 (2021)
539 139–146.
 - 540 [9] M. Hilal, C. Berthin, L. Martin, H. Azami, A. Humeau-Heurtier, Bidi-
541 mensional multiscale fuzzy entropy and its application to pseudoxan-
542 thoma elasticum, IEEE Transactions on Biomedical Engineering 67
543 (2020) 2015–2022.
 - 544 [10] A. Humeau-Heurtier, Texture feature extraction methods: A survey,
545 IEEE Access 7 (2019) 8975–9000.
 - 546 [11] L. E. Virgilio da Silva, A. C. Da Silva Senra Filho, V. P. S. Fazan, J. C.
547 Felipe, L. O. Murta, Two-dimensional sample entropy analysis of rat
548 sural nerve aging, in: 2014 36th Annual International Conference of
549 the IEEE Engineering in Medicine and Biology Society, 2014, pp.
550 3345–3348. doi:10.1109/EMBC.2014.6944339.
 - 551 [12] L. E. Silva, A. C. Senra Filho, V. Fazan, J. Felipe, L. Murta, Two-
552 dimensional sample entropy: assessing image texture through irregu-
553 larity, Biomedical Physics & Engineering Express 2 (2016) 045002.
 - 554 [13] C. Moore, T. Marchant, The approximate entropy concept extended to
555 three dimensions for calibrated, single parameter structural com-
556 plexity interrogation of volumetric images, Physics in Medicine &
557 Biology 62 (2017) 6092.

- 558 [14] A. S. F. Gaudêncio, P. G. Vaz, M. Hilal, J. M. Cardoso, G. Mahé,
559 M. Lederlin, A. Humeau-Heurtier, Three-dimensional multiscale
560 fuzzy entropy: validation and application to idiopathic pulmonary
561 fibrosis, *IEEE journal of biomedical and health informatics* 25 (2020)
562 100–107.
- 563 [15] A. S. Gaudêncio, P. G. Vaz, M. Hilal, G. Mahé, M. Lederlin,
564 A. Humeau-Heurtier, J. M. Cardoso, Evaluation of covid-19 chest
565 computed tomography: A texture analysis based on three-dimensional
566 entropy, *Biomedical Signal Processing and Control* 68 (2021)
567 102582.
- 568 [16] M. Rostaghi, H. Azami, Dispersion entropy: A measure for time-
569 series analysis, *IEEE Signal Processing Letters* 23 (2016) 610–614.
- 570 [17] H. Azami, L. E. V. da Silva, A. C. M. Omoto, A. Humeau-
571 Heurtier, Two-dimensional dispersion entropy: An information-
572 theoretic method for irregularity analysis of images, *Signal Process-
573 ing: Image Communication* 75 (2019) 178–187.
- 574 [18] M. Costa, A. L. Goldberger, C.-K. Peng, Multiscale entropy analysis
575 of complex physiologic time series, *Physical Review Letters* 89
576 (2002).
- 577 [19] S. C. G. Laboratory, Texture synthesis : Misc textures, ??? URL:
578 [https://graphics.stanford.edu/projects/texture/demo/synthesis_](https://graphics.stanford.edu/projects/texture/demo/synthesis_eero.html)
579 [eero.html](https://graphics.stanford.edu/projects/texture/demo/synthesis_eero.html), accessed july 2021.
- 580 [20] L.-Y. Wei, M. Levoy, Fast texture synthesis using tree-structured
581 vector quantization, in: *Proceedings of the 27th Annual Confer-
582 ence on Computer Graphics and Interactive Techniques, SIGGRAPH*
583 '00, ACM Press/Addison-Wesley Publishing Co., USA, 2000, pp.
584 479–488. URL: <https://doi.org/10.1145/344779.345009>. doi:10.1145/
585 344779.345009.
- 586 [21] H. Azami, J. Escudero, Amplitude- and fluctuation-based dispersion
587 entropy, *Entropy* 20 (2018).
- 588 [22] W. Chen, J. Zhuang, W. Yu, Z. Wang, Measuring complexity using
589 fuzzyen, apen, and sampen, *Medical Engineering & Physics* 31 (2009)
590 61–68.
- 591 [23] M. Labriffe, L.-M. Leiber, Diffusion, cartographie adc, effet t2 en irm
592 cérébrale : kézaco, *Journal d'imagerie diagnostique et intervention-
593 nelle* 2 (2019) 289–293.
- 594 [24] M. Zulfiqar, A. Shetty, R. Tsai, M.-H. Gagnon, D. M. Balfe, V. M.
595 Mellnick, Diagnostic approach to benign and malignant calcifications
596 in the abdomen and pelvis, *RadioGraphics* 40 (2020) 731–753. PMID:
597 32302263.